A G-quadruplex DNA for Fluorescent and Colorimetric Detection of Thallium(I)

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Abstract

Thallium is a highly toxic heavy metal, but its sensing is underexplored compared to its neighbouring elements in the periodic table: lead and mercury. Thallium has two oxidation states. A DNAzyme-based biosensor for Ti$^{3+}$ was reported recently, representing the first work in this area. However, the most environmentally abundant thallium is monovalent Ti$^{+}$, which is the focus of this work. Since Ti$^{+}$ is similar to K$^{+}$ in terms of size and charge, G-quadruplex DNAs are herein tested for Ti$^{+}$ detection. First, nine dual fluorophore labelled DNA probes are screened. Among them, a DNA designated PS2.M has the largest increase in the fluorescence resonance energy transfer (FRET) efficiency upon Ti$^{+}$ addition. This FRET-based assay is directly used as a biosensor yielding a detection limit of 59 $\mu$M Ti$^{+}$. In comparison, K$^{+}$ had a much lower response and the other tested monovalent metals do not produce a significant signal increase. In addition, a colorimetric sensor was developed based on DNA protected gold nanoparticles. When folded by Ti$^{+}$, the non-labelled PS2.M DNA cannot effectively adsorb onto gold nanoparticles. This leads to a color change from red to blue upon salt addition. The detection limit is 4.6 $\mu$M Ti$^{+}$, and Ti$^{+}$ spiked in a lake water sample can also be detected. CD spectroscopy is used to further understand Ti$^{+}$ binding to PS2.M. This study demonstrates that DNA can also be used for detecting Ti$^{+}$, and this work gives rise to a highly effective probe for this purpose.

Keywords: thallium, DNA, fluorescence, FRET, gold nanoparticles, biosensors
Thallium is a trace element with extremely high toxicity.\textsuperscript{1,2} Since its discovery, thallium has been identified as the source of poisoning for many intentional and unintentional deadly incidences.\textsuperscript{3,4} Like most heavy metals, thallium enters the environment often as a by-product of mining.\textsuperscript{5} It is estimated that over 2000 tons of thallium are generated by industrial processes annually.\textsuperscript{6} Additionally, soluble thallium ions can travel deep into soil and be absorbed by crops. Currently, thallium is used in the production of superconductive materials, which has raised growing environmental concerns.

Normal drinking water should contain less than 2.5 to 10 nM thallium as regulated by the US Environmental Protection Agency, while groundwater can routinely reach ~100 nM. Concentrations of 1–88 ppm (5-440 µM) thallium are reported in river areas for metal mining drainage.\textsuperscript{2} Thallium has two oxidation states. In the environment, thallium exists almost exclusively in the monovalent Tl\textsuperscript{+} state, making detection of Tl\textsuperscript{+} even more analytically relevant. It has been noted for decades that Tl\textsuperscript{+} resembles K\textsuperscript{+},\textsuperscript{7} which is postulated to be a reason for its toxicity. Tl\textsuperscript{+} and K\textsuperscript{+} have similar ionic radii (Tl\textsuperscript{+}: 1.54 Å, K\textsuperscript{+}: 1.44 Å), the same charge, and can substitute each other in minerals and some biological reactions. For example, Tl\textsuperscript{+} can replace Na\textsuperscript{+} and K\textsuperscript{+} in the glutamate transporter excitatory amino acid carrier,\textsuperscript{8} and in quadruplex DNA.\textsuperscript{9,10}

While its toxicity is higher than lead, cadmium and even mercury, thallium is often less studied. This is partially attributable to the lack of analytical methods that can accurately measure thallium.\textsuperscript{2} While thallium can be analyzed by a variety of techniques including inductively-coupled plasma mass spectroscopy (ICP-MS), differential pulse anodic stripping voltammetry, and atomic absorption spectrophotometry,\textsuperscript{11} its volatility makes detection more challenging than other metals. In this regard, low-cost biosensors are an attractive solution for its analysis.
Among the various types of biomolecules available for biosensor development, DNA is highly attractive due to its excellent programmability, versatility in metal coordination, and high stability.\textsuperscript{12-15} DNA-based biosensors for many heavy metals have been reported, including Pb\textsuperscript{2+},\textsuperscript{16-18} Hg\textsuperscript{2+},\textsuperscript{15,19} Ag\textsuperscript{+},\textsuperscript{20} Cd\textsuperscript{2+},\textsuperscript{21} Cu\textsuperscript{2+},\textsuperscript{22} and trivalent lanthanide ions.\textsuperscript{23,24} However, thallium detection has not been explored until very recently. We reported a method for detecting Tl\textsuperscript{3+} using an RNA-cleaving DNAzyme and a phosphorothioate (PS)-modified substrate.\textsuperscript{25} This DNAzyme is inactive with the PS substrate. Tl\textsuperscript{3+} can desulfurize the substrate, thus converting the inactive PS substrate into the active form to yield a fluorescence signal. However, this sensor has no response to Tl\textsuperscript{+}. We previously tested a low concentration of Tl\textsuperscript{+}, and here up to 1 mM Tl\textsuperscript{+} was tested (Figure S1) and still no response was observed. It is speculated that the thiophilicity of Tl\textsuperscript{+} is much lower than that of Tl\textsuperscript{3+} and thus cannot desulfurize the PS-modified substrate. While it is possible to oxidize Tl\textsuperscript{+} to Tl\textsuperscript{3+}, a direct detection method is more desirable.

Since Tl\textsuperscript{+} is similar to K\textsuperscript{+}, and K\textsuperscript{+} is able to stabilize guanine quadruplex DNA structures, we herein explore whether quadruplex-forming DNAs can be harnessed for Tl\textsuperscript{+} detection. Indeed, we discovered a DNA sequence that has higher affinity for Tl\textsuperscript{+} than for K\textsuperscript{+} and designed both fluorescent and colorimetric sensors.

**Materials and Methods**

**Chemicals.** All the dual-labelled DNA samples were from Gene Link (Hawthorne, NY). The non-labelled DNAs were from Eurofins (Huntsville, AL). TlCl, TlCl\textsubscript{3}, LiCl, NaCl, KCl, RbCl, CsCl, and NH\textsubscript{4}Cl were from Sigma-Aldrich. These metal salts were dissolved in 5 mM HEPES (pH 7.6) to make 13.25 mM stock solutions. 4-(2-Hydroxyethyl)piperazine-1-ethanesulfonic acid (HEPES)
was from VWR. The 13 nm gold nanoparticles (AuNPs) were prepared via the citrate reduction method as described previously,\textsuperscript{26} and the initial AuNP concentration was determined to be 13 nM.

**FRET-based detection.** FRET-based detection was performed in a $1 \times 1$ cm quartz fluorescence cuvette using a Cary Eclipse fluorometer. All titration tests began with a 3 mL solution containing 5 mM HEPES (pH 7.6), and 20 nM of DNA. The goal was to monitor the relative change of the two emission peaks with different metal ions. A metal stock solution (13.25 mM) was gradually titrated into the sample and the excitation wavelength of 495 nm was used (emission from 510 to 630 nm). The ratiometric response was calculated by dividing the fluorescence intensity at 585 nm over that at 518 nm. Experiments were performed in triplicate. For kinetic experiments, a final of 2.35 mM TlCl was added and the 585 nm emission intensity was monitored at 12 sec intervals. For the KCl kinetics, the emission at 518 nm was monitored. For the interference tests, the starting solution already contained a competing analyte (2.87 mM), and then 50 µL of the TlCl stock solution was added to measure the response. TlCl$_3$ stock (100 mM) was prepared in 1% HCl. At this concentration, it is not completely soluble. The suspension was agitated and then quickly diluted in Milli-Q water to make 5 mM and 0.1 mM solutions (full solubility achieved under these dilute and acid conditions). Then these stocks were added to the sensor in 5 mM HEPES (pH 7.6).

**Colorimetric detection.** Colorimetric detection was performed by first mixing 3 µL DNA (100 µM), 3 µL metal stock solution (13.25 mM), and 9 µL of HEPES buffer (5 mM, pH 7.6). After 1 min, 200 µL of AuNP solution was added to the mixture, followed by adding 100 µL NaCl (200 mM). The final concentrations for DNA, metal analyte, AuNPs, and added NaCl were 0.95 µM, 0.13 mM, 8.25 nM, and 63.49 mM respectively. The color of AuNPs changes to blue upon salt addition if not protected by DNA adsorption. The color of AuNPs was recorded by a digital camera. UV-vis absorption was measured in a 1 cm quartz cuvette using an Agilent 8453 spectrometer.
The UV-vis spectra were recorded 5 min after mixing AuNPs with NaCl. The ratiometric response was calculated by dividing the absorbance intensity at 650 nm by that at 520 nm. Experiments were performed in triplicate. Lake water experiment was performed by mixing 3 µL DNA (100 µM), 0.75 µL metal solution, and 11.25 µL Lake Ontario water (no extra HEPES buffer added here). This mixture was added to 200 µL of AuNP and then 100 µL NaCl (200 mM) with 5 mM HEPES buffer (pH 7.6) was added. The Tl⁺ concentration refers to the concentration before adding AuNPs.

**CD spectroscopy.** CD spectroscopy was performed in a 1 cm UV-vis quartz cuvette using a Jasco J-715 Spectrophotometer. Prior to each experiment, a 5 mM HEPES (pH 7.6) solution was measured as blank. For each experiment, 200 µL of non-labeled DNA (7.5 µM) in 5 mM HEPES (pH 7.6) was used. Then a metal salt was added to induce DNA folding. Measurements were performed using a continuous scanning mode (100 nm/min) from 220 nm to 330 nm, and a sensitivity of 100 mdeg. The buffer blank was subtracted from the measured signals. Other settings included a 0.5 nm data pitch, 1 sec response, and 1.0 nm bandwidth. The average from three scans was plotted.

**Results and Discussion**

**Screen of a G-quadruplex DNA.** Due to the similarity between Tl⁺ and K⁺, we hypothesize that Tl⁺ might selectively fold some guanine-rich DNA. This DNA conformational change may be utilized for its detection. Due to the limited understanding of thallium/DNA interactions,²⁷,²⁸ it is difficult to rationally design an oligonucleotide to test our hypothesis. Therefore, we screened a few common quadruplex-forming sequences. We employed a fluorescence resonance energy transfer (FRET)-based assay for this screen, so that an optimal sequence can be directly used as a
biosensor. These DNAs were labeled at their two termini with a FAM (carboxyfluorescein) and a TMR (tetramethylrhodamine), respectively. Tl⁺-induced folding might reduce the end-to-end distance and thus increase the FRET efficiency (Figure 1A). FAM is the FRET donor, transferring its energy to the nearby TMR acceptor, and the FRET efficiency depends on the inter-fluorophore distance. In this study, a total of six G-rich DNAs were used (Figure 1B). For example, the PS2.M DNA was originally identified as an aptamer for binding hemin, while K⁺-Apt is from a previous paper used for sensing K⁺. AS1411 is an aptamer targeting nucleolin on cancer cells, while AS1411-6 contains two more guanine repeating units based on AS1411. In addition, three control sequences were also included for comparison (the last three sequences in Figure 1B). Ade-Apt-FT is the adenosine aptamer, Hg-Apt-FT binds Hg²⁺, and Ctrl-DNA-FT is a random sequence without known molecular binding property.

Figure 1. (A) A scheme showing Tl⁺-induced DNA conformational change into a G-quadruplex and the accompanying enhanced FRET efficiency. (B) DNA sequences and modifications used in

<table>
<thead>
<tr>
<th>Name</th>
<th>DNA Sequence (5' to 3')</th>
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<tbody>
<tr>
<td>PS2.M-FT</td>
<td>FAM-GTGGTAGGGCAGGGTGGTGG-TMR</td>
</tr>
<tr>
<td>PW17-FT</td>
<td>FAM-GGTTAGGGCGGTTGGG-TMR</td>
</tr>
<tr>
<td>T30695-FT</td>
<td>FAM-GGTTAGGGCGGTTGGG-TMR</td>
</tr>
<tr>
<td>K⁺-Apt-FT</td>
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</tr>
<tr>
<td>AS1411-FT</td>
<td>FAM-GTGGGTTGGGTTGGGTTGGGTTGGG-TMR</td>
</tr>
<tr>
<td>AS1411-6-FT</td>
<td>FAM-GTGGGTTGGGTTGGGTTGGGTTGGGTTGGG-TMR</td>
</tr>
<tr>
<td>Ade-Apt-FT</td>
<td>FAM-ACCTGGGAGATTTGCGCAGGAAGG-TMR</td>
</tr>
<tr>
<td>Hg-Apt-FT</td>
<td>FAM-TTCTTTTCTTCCCTTGGTGGTGGTGGTGGTGG-TMR</td>
</tr>
<tr>
<td>Ctrl-DNA-FT</td>
<td>FAM-ACGCATCTGTGAGAGAGAACCTGGA-TMR</td>
</tr>
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this work for the FRET-based probe screening. The first six are G quadruplex-forming DNAs, and the last three are controls for comparison.

We first scanned the steady-state fluorescence emission spectra of these nine DNAs in the presence and absence of Ti\(^{+}\). For example, the black spectrum in Figure 2A was obtained by exciting the PS2.M-FT DNA at 492 nm, yielding two peaks at 518 nm and 585 nm, respectively. The 518 nm peak is from the FAM emission and the 585 peak is mainly due to energy transfer from FAM to TMR. After adding Ti\(^{+}\), the FAM peak dropped significantly, while the TMR peak increased concomitantly, indicating that Ti\(^{+}\) can shorten the distance between these two fluorophores. Therefore, this DNA might be a good probe for Ti\(^{+}\) based on the scheme in Figure 1A. When the same concentration of K\(^{+}\) was added (Figure 2B), the FAM peak dropped only slightly and the TMR peak lacked the correlated increase. This suggests either a weaker binding affinity or a different way of DNA folding occurring when interacting with K\(^{+}\). This difference is useful for the distinction of these two ions.

The same experiment was performed using all the other DNA sequences, and the emission intensity ratios of the two peaks before and after adding Ti\(^{+}\) were plotted (Figure 2C). The initial FRET efficiency is quite different for these nine DNAs (the black bars), indicating that they have a broad range of end-to-end distance distribution. All the sequences have higher FRET efficiency after adding Ti\(^{+}\), indicating DNA folding and shorter end-to-end distance. Most G-rich DNA displayed an obvious FRET change, while the control DNAs changed to a lesser extent. An ideal probe should have a large signal change by Ti\(^{+}\), and we conclude that PS2.M-FT is an optimal
sequence among the ones we tested (yielding 3.4-fold signal change). The K+-Apt DNA has the second highest response (2.6-fold).

We then studied the kinetics of signalling upon metal addition. After monitoring the background fluorescence for 2 min, Tl⁺ was added and the rise of the 585 nm peak followed the first-order reaction kinetics with a rate constant of 2.6 min⁻¹ (Figure 2D, red triangles). It took ~1 min for the signal to stabilize. For comparison, K⁺ induced a faster signal change (black dots). The drop of the 518 nm peak followed a rate constant of 7.5 min⁻¹, and a stable signal was achieved in just 12 sec. It was reported that Tl⁺ binds to halides such as chloride more tightly than K⁺ does. This may explain its slower kinetics in binding to DNA, since the associated Cl⁻ ligands need to be displaced before Tl⁺ entering the G-quadruplex cavity. Overall, the kinetics is sufficiently fast for analytical applications.

Figure 2. The PS2.M-FT fluorescence emission spectra before and after adding a final concentration of (A) 2.36 mM TlCl, or (B) adding the same concentration of KCl. Reaction buffer:
5 mM HEPES pH 7.6 with 20 nM PS2.M-FT DNA. (C) Response of the various DNA probes to Tl⁺. The ratios of the two fluorescence peaks are plotted. (D) Kinetics of the increase of the 585 nm peak of PS2.M after adding Tl⁺ and the drop of the 518 nm peak after adding K⁺.

**FRET-based Tl⁺ detection.** Since PS2.M-FT has the highest response to Tl⁺ among all the tested DNAs, we further studied it for Tl⁺ detection. First, metal selectivity was measured. We monitored the fluorescence ratio as a function of concentration of each monovalent cation (Figure 3A). Indeed, Tl⁺ has the highest response followed by K⁺. At 2.4 mM, Tl⁺ has a ratio greater than 1.8, while K⁺ is below 0.9 (note that the background value is ~0.6). The other ions did not show a significant response and their signal remained as the background level. This suggests that the signal change is likely due to G-quadruplex formation, since Tl⁺ and K⁺ are the most efficient for this reaction. Next, an interference assay was carried out, where the DNA probe was first incubated with each competing metal, followed by adding Tl⁺ (Figure 3B). In all the samples, Tl⁺ produced a significant signal increase. Therefore, these metal ions do not interfere with Tl⁺ detection. We also tested the response of this probe to Tl³⁺ (Figure 3C); the ratio remained unchanged with up to 16 μM Tl³⁺, which is consistent with the lack of strong interaction between Tl³⁺ and DNA. Tl³⁺ started to precipitate at even higher concentrations and thus was not further measured.

Some divalent metal ions, especially Pb²⁺, are also highly potent in stabilizing G-quadruplex. For this particular PS2.M DNA, Pb²⁺ was reported to be also a strong binder. We titrated Pb²⁺ into the PS2.M-FT DNA, but only observed fluorescence quenching of both fluorophores with no indicating of enhanced FRET (Figure S2). It is likely that the DNA folds into a different conformation with Pb²⁺, which is also supported by the previous work.
After confirming selectivity, we then measured sensitivity. Figure 3A shows that the dynamic range goes up to ~ 1 mM Tl\(^+\). After that, the signal change becomes much smaller. We then did a finer titration at lower metal concentrations up to 300 \(\mu\)M Tl\(^+\), and a linear relationship was observed (Figure 3D). By calculating the slope of this line and the standard deviation of background variation (\(\sigma\)), the detection limit is 59 \(\mu\)M Tl\(^+\) using \(3\sigma/\text{slope}\).

**Figure 3.** (A) The PS2.M-based sensor selectivity test at various metal concentrations. (B) A competitive test. The concentration of the competing salts is 2.87 mM and then a final concentration of 0.22 mM Tl\(^+\) is added. All the experiments are run in triplicate in 5 mM HEPES buffer (pH 7.6) with 20 nM DNA probe. (C) Response of the sensor to Tl\(^{3+}\). (D) Sensor sensitivity test at low Tl\(^+\) concentrations.
Colorimetric detection. While FRET is a sensitive method, the cost of dual-labeled DNA probes is relatively high and the detection still requires a fluorometer. To further improve the sensing method, we also aimed to design a colorimetric biosensor using this Tl⁺-induced DNA folding. Gold nanoparticles (AuNPs) are particularly attractive for this purpose since they have extremely high extinction coefficients and aggregation-induced color change.\textsuperscript{36-38} Dispersed AuNPs have an intense red color due to the surface plasmon effect. It has been well established that the rate of DNA adsorption by citrate-capped AuNPs is a strong function of DNA conformation.\textsuperscript{39-41} DNAs without stable secondary structures are more efficiently adsorbed and thus allow higher colloidal stability of AuNPs against salt-induced aggregation (Figure 4A). If the DNA is folded by Tl⁺ to inhibit its adsorption, AuNPs are more easily aggregated by the added salt and thus change color to blue. This method has been used to detect a diverse range of analytes by using DNA aptamer probes.\textsuperscript{42-44}

To test this sensing mechanism, we respectively incubated the non-labeled PS2.M DNA with Tl⁺ as well as other monovalent metal ions. Then citrate-capped 13 nm AuNPs were added followed by the addition of a concentrated NaCl solution. The resulting color was documented by a digital camera (Figure 4B). Indeed, we observed an intense purple color for the Tl⁺ sample, while all the other samples remained red as the control without any pre-incubated monovalent metal ions. It appears that the free PS2.M DNA was efficiently adsorbed by the AuNPs in the absence of Tl⁺, since it can protect the AuNPs. Tl⁺ inhibits this protection, which is consistent with the mechanism in Figure 4A. This successful colorimetric detection adds further weight to the hypothesis that PS2.M has in fact a high binding affinity towards Tl⁺. The UV-vis spectra of the AuNP samples with and without Tl⁺ are shown in Figure 4C, where a clear shift of the 520 nm peak to longer
wavelength is observed for the Tl$^+$ added sample. The increase in 650 nm extinction and decrease at the 520 nm peak upon Tl$^+$ addition allows for the ratiometric measurement (Figure 4D); the Tl$^+$ containing sample has the highest ratio, while the other samples are at the background level.

**Figure 4.** (A) A scheme of colorimetric sensor design. The PS2.M DNA is folded by Tl$^+$, retarding its adsorption by AuNPs, leading to AuNP aggregation by salt, and resulting in a color change to blue. Without Tl$^+$, the AuNPs are protected by the DNA. (B) Sensor color response to 2.65 mM various monovalent metal ions. (C) UV-vis spectra of the sensor samples with and without 2.65 mM Tl$^+$. (D) Quantification of the color change based on the extinction ratio at 650 nm over 520 nm. The DNA and metal ions were mixed in a 5 mM HEPES (pH 7.6) buffer. The final reagent
concentrations were PS2.M DNA = 0.95 µM, AuNP = 8.3 nM, NaCl = 64 mM, and TI⁺ or other metal ions = 0.13 mM. The final volume was 315 µL. (E) The response of the colorimetric sensor to various TI⁺ concentrations. (F) A UV-vis based ratiometric quantification of TI⁺ titration using the PS2.M or A₁₅ DNA. The listed TI⁺ concentration is before adding AuNPs and salt. After adding, the TI⁺ is diluted by ~30-fold.

Having demonstrated the feasibility and selectivity of this colorimetric sensor, the sensitivity was measured next. A gradual color progression from red to purple and then blue was observed with increasing of TI⁺ concentration (Figure 4E). Using UV-vis spectroscopy, the color change was quantified (Figure 4F, red dots), and this sensor can detect up to ~100 µM TI⁺. The detection limit was 4.6 µM TI⁺. Therefore, this colorimetric sensor is even more sensitive than the above FRET-based detection. With more than 10 µM TI⁺, the color change can be readily observed by the naked eye. As a control to confirm the sensing mechanism, the same experiment was repeated using an A₁₅ DNA (i.e. 15 adenines). The visual results showed that TI⁺ had little effect on the color of AuNPs and all the samples remained red (data not shown). The UV-vis spectroscopy tests showed minimal response towards TI⁺ as well (Figure 4F, blue dots). Therefore, it is the specific binding between TI⁺ and PS2.M responsible for the observed color change.

**CD Spectroscopy.** It is interesting to see that TI⁺ and K⁺ gave different responses in both the FRET and the colorimetric assays. To further understand metal binding, we characterized the folding of the DNA using circular dichroism (CD) spectroscopy. The DNA was dissolved in 5 mM HEPES buffer, the same as our sensing condition. In this buffer, the free PS2.M DNA showed two positive peaks at 250 nm and 295 nm, and a negative peak at 264 nm (Figure 5A, black spectrum). These features agree with the group III anti-parallel quadruplex structure. Our 5 mM HEPES buffer
already contained 2.5 mM Na\(^+\) at pH 7.6, and it appears that a fraction of the DNA was already folded by this background Na\(^+\).\(^{46}\) After adding Tl\(^+\), the two positive peaks increased and the negative peak slightly decreased. Therefore, Tl\(^+\) has shifted the equilibrium and folded more DNA into the quadruplex. Note that unfolded DNA does not generate much CD signal and the stronger signal can only be attributed to a greater amount of DNA being folded. Adding K\(^+\) only raised the 290 nm positive peak (Figure 5B), while adding Na\(^+\) did not change the folding of this DNA (Figure 5C). The FRET study and the CD data both indicate that Tl\(^+\) is the most efficient in folding the PS2.M DNA.

![Figure 5. CD spectra of the PS2.M DNA (7.5 µM) before and after adding 0.22 mM (A) Tl\(^+\), (B) K\(^+\), and (C) Na\(^+\).](image)

**Conclusions**

In summary, we screened multiple G-quadruplex DNAs using a FRET-based assay for Tl\(^+\) detection. Of these sequences, the PS2.M DNA was selected due to its significant change in the FRET efficiency upon Tl\(^+\) binding. While the signaling kinetics for Tl\(^+\) is ~3-fold slower than that for K\(^+\), it reaches a stable signal in 1 min. This sensor has a detection limit of 59 µM Tl\(^+\). Further
TL⁺-induced DNA conformational change and binding was characterized by CD spectroscopy, indicating a significant difference between TL⁺ and the rest of the monovalent metal ions in promoting the DNA folding into G-quadruplex. We further designed a colorimetric sensor using the same DNA sequence but without any fluorescence label. The PS2.M DNA adsorption by AuNPs was inhibited by TL⁺ due to DNA folding, and a red-to-blue color change was observed upon salt addition. The colorimetric detection method has a detection limit of 4.6 µM TL⁺. These detection limits are unlikely to be enough for monitoring drinking water, which requires detection of lower than 10 nM TL⁺. On the other hand, many mining related regions contain much higher TL⁺ and these sensors fit in the detection range of those applications. For drinking water monitoring, sample enrichment or oxidation to TL³⁺ might be needed. This is the first report on DNA-based sensor for TL⁺ detection, and it has enhanced our understanding on TL⁺/DNA interactions.

**Supporting Information**

The Supporting Information is available free of charge on the ACS Publication website at DOI: DNAzyme-based assay of TL⁺ and TL³⁺ at high metal concentrations, sensor response to Pb²⁺, and sensor response in Lake Ontario water. (PDF)

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